EMG evaluation of hip adduction exercises for soccer players: implications for exercise selection in prevention and treatment of groin injuries

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ABSTRACT
Introduction Exercise programmes are used in the prevention and treatment of adductor-related groin injuries in soccer; however, there is a lack of knowledge concerning the intensity of frequently used exercises. Objective Primarily to investigate muscle activity of adductor longus during six traditional and two new hip adduction exercises. Additionally, to analyse muscle activation of gluteals and abdominals. Materials and methods 40 healthy male elite soccer players, training >5 h a week, participated in the study. Muscle activity using surface electromyography (sEMG) was measured bilaterally for the adductor longus during eight hip adduction strengthening exercises and peak EMG was normalised (nEMG) using an isometric maximal voluntary contraction (MVC) as reference. Furthermore, muscle activation of the gluteus medius, rectus abdominis and the external abdominal obliques was analysed during the exercises. Results There were large differences in peak nEMG of the adductor longus between the exercises, with values ranging from 14% to 108% nEMG (p<0.0001). There was a significant difference between legs in three of the eight exercises (35–48%, p<0.0001). The peak nEMG results for the gluteals and the abdominals showed relatively low values (5–48% nEMG, p<0.001). Conclusions Specific hip adduction exercises can be graded by exercise intensity providing athletes and therapists with the knowledge to select appropriate exercises during different phases of prevention and treatment of groin injuries. The Copenhagen Adduction and the hip adduction with an elastic band are dynamic high-intensity exercises, which can easily be performed at any training facility and could therefore be relevant to include in future prevention and treatment programmes.

INTRODUCTION
Groin injuries are one of the most common types of injuries in soccer accounting for 8–18% of all injuries.1–7 It is described that the typical groin injury in soccer is primarily related to the hip adductors, which account for 69% of all groin injuries.3 There is consistent evidence that previous groin injury increases the risk for subsequent groin injury.1 5 9 10 A common assumption is that strength deficits due to inadequate rehabilitation is a possible reason for previous injuries being a risk factor.1 5 9 Additionally, reduced hip adductor strength has been found to be a risk factor for subsequent groin injury.2 9 11 Therefore, hip adduction strengthening exercises seem to have a large potential in both the prevention and treatment of groin injuries.

Currently, no studies have been able to demonstrate a reduction in the number of groin injuries in soccer.12–14 Various explanations for this have been proposed, such as insufficient compliance,12–14 over-optimistic effect sizes12 and inadequate exercise intensity.12 Physical training has proven effective in the treatment of long-standing adductor-related groin pain,13 which is supported by other studies showing favourable outcomes of exercise interventions.15 None of the aforementioned studies12–15 17–20 however, account for the intensity of the included exercises, that is, relative load, perceived exertion or muscle activity. Consequently, no information exists on the specific intensity of exercises in the treatment of groin pain in athletes. In this regard, electromyography is a pertinent method of evaluating exercise intensity.21–24 The results of the present study could therefore be used to optimise future training programmes by a greater understanding of exercise intensity when selecting exercises to match different contextual situations and physiological demands in prevention and treatment of adductor-related groin injuries.

The primary purpose of this study was therefore to examine the muscle activity, defined as the peak normalised EMG signal (nEMG) of the adductor longus during six traditional and two new hip adduction strengthening exercises. Additionally, muscle activity of the gluteus medius, rectus abdominis and external abdominal oblique was evaluated.

MATERIALS AND METHODS
Subjects
Forty healthy male elite soccer players older than 18 years participated in the study (21.4±3.3 years, 182.4±7.9 cm, 77.8±7.9 kg). The participants were recruited on a voluntary basis through coaches and physiotherapists from teams from the Danish Senior 1st Division, 2nd Division and the Under-19 League. All participants were training >5 h per week with 1–2 weekly matches. Players were eligible for inclusion if they did not have current hip or groin symptoms and/or injury or other injuries which could be presumed to influence the execution of the tests. As a large proportion of soccer players experience mild hip and groin symptoms and disability, that may not be perceived as problematic by the player, a score higher than 80 out of 100 in the subscale ‘function, sports and recreational activities’ from the Copenhagen Hip and Groin Outcome Score,25 HAGOS (Sport), was required. Furthermore, we
decided to exclude players if they reported pain >2 on a numeric pain rating scale in the Adductor Functional Pain Test during maximal voluntary contractions (MVCs) and during the performance of the eight exercises. Inclusion of participants ended when the desired sample size was reached. No exercise or training was allowed on the same day before testing and all participants gave written informed consent according to the Helsinki Declaration before testing was initiated. The study was approved by the Danish National Committee on Health Research Ethics (H-3-2011-145).

Testing procedure
The participants attended two separate test sessions. On the first session, they performed a 10 min standardised warm-up and were subsequently familiarised with all the exercises. The second session was conducted with a minimum of 3 days’ interval to avoid delayed onset muscle soreness (DOMS). After the warm-up, the players performed the MVC tests followed by the eight exercises.

Hip adduction exercises
The present study included six traditional hip adduction exercises and two new exercises which were considered to activate the hip adductor muscle group with a different intensity (figure 1). We wanted to introduce exercises that we thought would represent both high and low intensities, as this can be useful in clinical situations, such as acute versus chronic conditions, where muscle-tendinous structures need to be targeted with different intensities. Only exercises where the hip adductors were used as a prime mover in hip adduction were included to ensure similar muscle actions in our comparisons. The preferred kicking leg was defined as the dominant leg and was used as the training leg when performing the exercises.

The exercises were performed in a randomised order and a minimum of 30 s break was held between the exercises. EMG increases due to fatigue with consecutive repetitions within a set performed to failure, but not between consecutive sets with rest periods in between. To avoid fatigue, the subjects therefore performed two separate sets and the dynamic exercises were performed with three repetitions and one repetition for the isometric exercises in each set. All exercises were performed for 6 s per repetition: 3 s concentric and a 3 s eccentric contraction for the dynamic exercises, with a gradual increase and decrease of tension for the six second isometric exercises.

For the two exercises that can be adjusted using an external load, the hip adductor machine and the hip adduction with an elastic band, a relative load of 10 repetition maximum (RM), was chosen. The load on the machine and the resistance of the elastic bands (number and strength of the elastic bands and distance from the fixation point) were individually determined on the first session. The participants subjectively evaluated the exercises after 5–6 repetitions and adjusted the load accordingly. Ten repetitions were performed and the relevant load was noted if participants considered the load equivalent to 10 RM. A load of 10 RM is described as heavy resistance training and has been used previously in hip adduction strengthening and therefore it is considered as an appropriate reference for exercise comparisons.

The eight exercises
(a) Isometric adduction—with a ball between the ankles (IBA): Isometric hip adduction against a football placed between the feet inferior to the medial malleoli when lying supine. The knees are kept straight and feet vertical.
(b) Isometric adduction—with a ball between the knees (IBK): Isometric hip adduction against a football placed between the knees when lying supine with hips and knees flexed and feet flat on the surface. The first toe is pointed straight forward and the knees are pressed against the ball as hard as possible. Exercise used in refs. 12 15 28.
(c) Side-lying hip adduction (SLA): The player is lying on the side of the dominant leg with the dominant leg straight and the non-dominant leg flexed 90° in the hip and knee. Maximal hip adduction of the dominant leg is performed.

Figure 1 The eight included hip adduction exercises: (a) isometric adduction with a ball between the ankles; (b) isometric adduction with a ball between the knees; (c) side-lying adduction; (d) sliding hip adduction/adduction exercise; (e) hip adduction with an elastic band; (f) hip adductor machine; (g) supine bilateral hip adduction; (h) Copenhagen adduction.
keeping the knee straight and foot horizontal. Exercise used in ref. 15. 

(d) **Sliding hip abduction/adduction** (SLIDE): Standing with the dominant leg on a wash cloth with hips and knees straight and hands placed laterally on the trunk. The dominant leg is abducted, so the centre of gravity moves laterally as much as controllably possible. The dominant leg is then adducted, sliding back to the starting position. Exercise modified from refs. 15, 28.

(e) **Hip adduction with an elastic band** (EB): Standing with the hip of the dominant leg positioned in maximal abduction. An elastic band (Thera-Band) is attached to a fixation point and around the ankle of the dominant leg keeping a slight tension in the elastic band from the beginning. The upper body is kept straight and the player holds on to a stable support. The dominant leg is adducted until there is a foot width between the feet and the dominant leg is approximately half a foot length behind the foot of the non-dominant leg. Exercise modified from refs. 15, 27, 28.

(f) **Hip adductor machine** (AM): Sitting in a hip adduction machine, ‘Adductor’ (TechnoGym, Bologna, Italy), with a slight knee flexion holding on to the handles. The legs are then moved into maximal hip abduction and back. Exercise used in ref. 28.

(g) **Supine bilateral hip adduction** (SBA): Supine with the hips in 90° flexion and the knees in 45° flexion. The legs are moved into maximal hip abduction and back keeping the flexion in the hips and knees constant. New suggested low-intensity exercise.

(h) **Copenhagen Adduction** (CA): A partner exercise where the player is lying on the side of the non-dominant leg with one forearm as support on the floor and the other arm placed along the body. The dominant leg is held in approximately the height of the hip of the partner, who is holding the leg with one hand supporting the ankle and the other supporting the knee. The player then raises the body from the floor and the non-dominant leg is adducted so that the feet touch each other and the body is in a straight line. The body is then lowered halfway to the ground while the foot of the non-dominant leg is lowered so that it just touches the floor without using it for support. New suggested high-intensity exercise.

**Electromyography**

Bipolar disposable silver/silver chloride (Ag/AgCl) surface electrodes (White Sensor, Ambu A/S, Ballerup, Denmark) were used bilaterally to collect data from the adductor longus, gluteus medius, rectus abdominis and the external abdominal oblique. The electromyography (EMG) activity was sampled at 1024 Hz using two sets (4 channels each) of the Nexus 10 data loggers (Mind Media, The Netherlands) and digitally converted at a 24 bit resolution using integrated A/D-converters. To reduce impedance, the area where the electrodes were placed was shaved and cleansed with an abrasive gel (Acqua gel, Meditec, Parma, Italy).

**Electrode placement**

The electrodes were placed parallel to the muscle fibres with an inter-electrode distance of 2 cm to avoid unstable recordings due to tendon and motor endplate effects, as recommended by the SENIAM project. To confirm the correct placement of electrodes, a manual muscle test was used and the EMG signal was checked on a laptop via Bluetooth. The same tester conducted preparation and control for all participants, and electrodes were placed in the following way:

**Adductor longus:** medially on the thigh equivalent to the proximal third of the distance from the pubic tubercle to the insertion on the femur.

**Gluteus medius:** half the distance between the iliac crest and the major trochanter anterosuperiorly from the Gluteus Maximus.

**Rectus abdominis:** half the distance between the umbilicus and the pubic symphysis and centred on the muscle belly, that is, 2–4 cm laterally from the midline depending on the size of the participant. **External abdominal obliques:** directly below the most inferior point of the costae in direction towards the opposite pubic tubercle.

**Reference electrodes:** on the medial surface of the tibia. All electrodes were fixated with tape (Fixomull Stretch, BSNmedical, Germany).

**Reference contractions**

The participants performed two MVCs in six different test positions and in a randomised order to determine the maximal muscle activity. The trial with the highest EMG value was used as the reference contraction, that is, 100%, to normalise the peak EMG recordings from the exercises. MVCs lasted 5 s each and participants were given at least 30 s rest between each test. A standardised command was used during tests; ‘go ahead, push, push, push and relax’, which has been used previously in the evaluation of maximal strength recordings. MVCs were conducted in the following way:

**Adductor longus MVC:** a bilateral hip adduction was performed supine with the hips and knees straight and a ball placed between the knees. **Gluteus medius MVC:** a maximal hip abduction was performed side-lying with knees straight and the tested leg in 25° of hip abduction.

A strap belt around the knees just proximal of the lateral femur epicondyle was used as it has been shown to increase the reliability of maximal hip abduction measurements. A straight abdominal flexion in an ‘Abdominal Crunch R.O.M’ machine (TechnoGym, Bologna, Italy) and a trunk rotation in a ‘Rotary Torso’ machine (TechnoGym) to each side. Both MVCs were performed isometrically with the resistance and movement of the machines locked.

**Data extraction**

All raw EMG signals were digitally filtered by a Butterworth fourth-order high-pass filter (10 Hz cut-off frequency). Raw EMG was checked visually on a computer and processed to ensure correct signal registration. For each individual muscle, a moving root mean square (RMS) EMG (500 ms time constant) was used to identify peak EMG within each contraction (repetition) and normalised to the maximal moving RMS EMG (500 ms time constant) obtained during MVC. Reported peak nEMG for each exercise was calculated using the average of the peak nEMG from all repetitions, that is, six repetitions for the dynamic exercises and two repetitions for the isometric exercises.

**Statistical methods**

Intraclass correlation coefficient (ICC) model 3 was used to determine the intrasession reliability of the repetitions (six dynamic and two isometric) using the peak nEMG from all subjects in each exercise. As a reference, ICC values >0.75 were considered excellent and 0.40–0.75 fair to good. A repeated-measure one-way analysis of variance (ANOVA) was used for the evaluation of peak nEMG for each muscle with nEMG as...
the dependent variable and exercise as the independent variable. A post hoc analysis was made to compare the exercises and a Bonferroni correction was made to account for the risk of mass significance, that is, all p values presented have been multiplied by the relevant number of pairwise comparisons. When comparing differences between the adductor muscle activity of the two legs, a two-way ANOVA was used to test for muscle by exercise interaction, with nEMG as the dependent variable and muscle (dominant and non-dominant adductor longus) and exercise as independent variables. All nEMG values are reported as least square mean±SE and the level of significance was set at p<0.05.

Sample size calculation
The SD in nEMG for leg exercises has been shown to be approximately 15%.24 The minimal clinically relevant difference between exercises has been suggested to be 10% nEMG.22 45 With a power of 80% (β 0.80) and a significance level of 5% (α=0.05), the minimum number of participants was calculated to be 20. To account for multiple comparisons and missing data (eg, due to electrode errors etc.), we decided to include 40 participants.

RESULTS
Subjects
Data from two participants were missing due to broken reference electrodes. Therefore, the analysis included 38 participants (table 1). Full datasets were registered for 35 participants and data from three participants had a total of 18 single contraction measurements showing uncorrectable registration errors, which led to their exclusion from the respective analyses. Analysis of peak EMG values was therefore conducted to account for the missing values.

Reliability of repetitions
For the majority of the exercises, excellent ICC values were found between the repetitions for adductor longus (ICC 3=0.81–0.97). The ICC values for the dominant adductor longus in the isometric adduction with the ball between the knees and between the ankles were fair to good with an ICC of 0.59 and 0.74, respectively.

Peak muscle activity
We found a significant exercise by muscle interaction (ANOVA: p<0.0001) for the adductor longus, as well as a significant difference between the exercises for the gluteus medius, rectus abdominis and the external abdominal oblique muscles (ANOVA: p<0.0001). See table 2 for specifications.

Post hoc analysis
The post hoc analysis of adductor longus activation (table 3) showed that the supine bilateral hip adduction had significantly lower values than all other exercises (p<0.01). The side-lying hip adduction was significantly higher than the supine bilateral hip adduction and significantly lower than all the other exercises (p<0.01). Furthermore, there was a significant difference from the three exercises with the highest nEMG activity and the three lowest ranked exercises (p<0.05) (table 3).

Between-leg difference
Three of the exercises, the Copenhagen Adduction, the hip adduction with an elastic band and the side-lying hip adduction, had significantly higher adductor longus activation in the dominant leg (training leg) compared to the non-dominant leg (non-training leg), 35–48%, p<0.0001 (figure 2). Consequently, these exercises can be considered asymmetric regarding intensity.

DISCUSSION
The main purpose of this study was to evaluate the exercise intensity using sEMG to measure muscle activity during the hip adduction exercises frequently used in the prevention and treatment of adductor-related groin injuries. The findings of this study show that there is a significant difference in muscle activation between the included exercises.

This evaluation of exercise intensity can help guide clinical decision making by an increased understanding of ways to progress strength training exercises in the prevention and treatment of adductor-related injuries. The results show that seven exercises can be considered strength training, as they elicit an intensity higher than 60% of maximum, which is documented to be conducive of muscle strength gains.46 Furthermore, it could be assumed that it is possible to regulate the intensity of some of the exercises by changing the RM, both to a higher or lower relative load or by pressing submaximally on the ball in the isometric exercises.

There was no significant difference between the five exercises with the highest nEMG values. These exercises are all performed in different test positions and with different kinds of equipment (elastic band, machine, wash cloth, ball or without anything), allowing the clinician to choose the exercises which fit the players’ situation and preferences best. This also shows promising possibilities for implementing strength training on the pitch for football players, as the Copenhagen Adduction exercise, the hip adduction with an elastic band and the isometric hip adduction with a ball between the knees all can be performed at any training facility with a minimum of equipment needed. The optimal number of sets, repetitions and frequency of the exercises is, however, beyond the scope of this study.

There is limited research investigating adductor longus muscle activity during exercise. A review investigating the free barbell squat finds that a greater hip external rotation position, a wide stance of the feet, as well as an increased load will increase hip adduction activation during the exercise.47 The highest nEMG value found for the hip adductors was, however, only 23.1%.48 A different study, which investigated adductor longus activation during a single-leg squat, a lunge and a step up-and-over exercise, showed peak nEMG values at 15–19%, 8–21% and 15–22% nEMG, respectively.49 The relatively low nEMG results found in these exercises indicate that they probably do not sufficiently activate the adductors to achieve strength increases and hypertrophy. Consequently, seven exercises from the present study appear to be superior in that respect, as they all focus primarily on the hip adduction movement, thereby reaching greater levels of muscle activity.

The adductor muscle group’s main action is described to be adduction of the thigh in the open kinetic chain and stabilisation of the lower extremity in the closed kinetic chain.50 51 The variability of soccer play stresses the adductor muscle group in different situations with both the high running loads with

### Table 1 Baseline data for 38 participants

<table>
<thead>
<tr>
<th>Age</th>
<th>21.4±3.3 years</th>
</tr>
</thead>
<tbody>
<tr>
<td>Height</td>
<td>182.4±7.9 cm</td>
</tr>
<tr>
<td>Weight</td>
<td>77.8±7.9 kg</td>
</tr>
<tr>
<td>Adductor functional pain test</td>
<td>0±0</td>
</tr>
<tr>
<td>HAGOS (Sport)</td>
<td>95.8±5.7 points</td>
</tr>
</tbody>
</table>
strain in the following season by 17 times, an imbalance with a preseason hip adduction/abduction strength ratio demonstrated in a study of ice hockey players, where a muscular weakness of the hip adductor muscles was associated with muscle injuries. This was supported by a study showing that an 8-week progressive strengthening programme using a dynamic hip adduction exercise with an elastic band increased eccentric hip adduction strength by 13%.

These movements can result in large amounts of stretching of highly activated muscles (lengthening contractions), which are associated with muscle injuries. Additionally, these movements create large stabilisation requirements around the hip, which if inadequate might also be a risk factor for injury. This was demonstrated in a study of ice hockey players, where a muscular imbalance with a preseason hip adduction/abduction strength ratio less than 80% increased the risk of sustaining an adductor muscle strain in the following season by 17 times, emphasising the importance of ensuring adequate strength of the adductors.

The included dynamic exercises appear to be superior to the isometric exercises as they include the element of lengthening contractions, thereby preparing the muscle-tendinous structures for the requirements of soccer. Exercises where the adductor-longus muscle is working eccentrically seem important to consider, especially in prevention, as this resembles the situation where the muscle-tendinous structures are at the highest risk of injury. Three of the exercises, the Copenhagen Adduction, the hip adduction with an elastic band and the hip adductor machine, all include eccentric contractions and a high nEMG activity of the adductor longus. They might therefore be recommended as the potentially best exercises in the prevention of adductor-related groin injuries in soccer players, although future studies need to confirm a possible preventive effect. These findings are supported by a study showing that an 8-week progressive strengthening programme using a dynamic hip adduction exercise with an elastic band increased eccentric hip adduction strength by 13%.

Additionally, these movements are supported by a study showing that an 8-week progressive strengthening programme using a dynamic hip adduction exercise with an elastic band increased eccentric hip adduction strength by 13%.

A substantiating argument for the potential of dynamic high-intensity exercises for soccer players is that an exercise, matching the proposed injury mechanisms and with high muscle activity, has been able to significantly prevent another muscle-tendinous injury. This study includes the Nordic Hamstring exercise, which has shown a biceps femoris peak nEMG of 91%, and is performed eccentrically to match the deceleration phase of the leg during running/sprinting, where hamstring injuries are described to occur.

### Table 2 Peak normalised EMG measurements for all exercises and muscles

<table>
<thead>
<tr>
<th>Exercise</th>
<th>Adductor longus</th>
<th>Gluteus medius</th>
<th>External abdominal oblique</th>
<th>Rectus abdominis</th>
</tr>
</thead>
<tbody>
<tr>
<td></td>
<td>Dominant side</td>
<td>Non-dominant side</td>
<td>Dominant side</td>
<td>Non-dominant side</td>
</tr>
<tr>
<td>1. Isometric adduction with a ball between the knees</td>
<td>108±6</td>
<td>102±6</td>
<td>10±3</td>
<td>25±3</td>
</tr>
<tr>
<td>2. Copenhagen adduction</td>
<td>108±5</td>
<td>69±6</td>
<td>20±3</td>
<td>48±3</td>
</tr>
<tr>
<td>3. Hip adduction with an Elastic band</td>
<td>103±6</td>
<td>70±6</td>
<td>18±3</td>
<td>18±3</td>
</tr>
<tr>
<td>4. Hip adductor machine</td>
<td>99±6</td>
<td>95±6</td>
<td>12±3</td>
<td>15±3</td>
</tr>
<tr>
<td>5. Sliding hip abduction/adduction exercise</td>
<td>98±6</td>
<td>89±6</td>
<td>36±3</td>
<td>45±3</td>
</tr>
<tr>
<td>6. Isometric adduction with a ball between the ankles</td>
<td>86±6</td>
<td>80±6</td>
<td>13±3</td>
<td>18±3</td>
</tr>
<tr>
<td>7. Side-lying hip adduction</td>
<td>64±6</td>
<td>17±6</td>
<td>22±3</td>
<td>14±3</td>
</tr>
<tr>
<td>8. Supine hip adduction</td>
<td>14±6</td>
<td>15±6</td>
<td>16±3</td>
<td>21±3</td>
</tr>
</tbody>
</table>

Values reported as mean peak normalised EMG± standard error in % of the MCV and listed in the order of adductor longus activation. Dominant side=side of the preferred kicking leg.

### Table 3 Pairwise comparisons adductor longus (dominant leg)

<table>
<thead>
<tr>
<th>Exercise</th>
<th>2. Copenhagen addition (108%)</th>
<th>3. Hip adduction with an elastic band (103%)</th>
<th>4. Hip adductor machine (99%)</th>
<th>5. Sliding hip adduction/adduction (98%)</th>
<th>6. Isometric adduction with a ball between the ankles (86%)</th>
<th>7. Side-lying hip adduction (64%)</th>
<th>8. Supine bilateral hip adduction (14%)</th>
</tr>
</thead>
<tbody>
<tr>
<td>1. Isometric adduction with a ball between the knees</td>
<td>0±5</td>
<td>5±5</td>
<td>9±5</td>
<td>10±5</td>
<td>22±5**</td>
<td>44±5**</td>
<td>94±5**</td>
</tr>
<tr>
<td>2. Copenhagen adduction</td>
<td>5±5</td>
<td>9±5</td>
<td>10±5</td>
<td>22±5**</td>
<td>44±5**</td>
<td>94±5**</td>
<td></td>
</tr>
<tr>
<td>3. Hip adduction with an elastic band</td>
<td>4±5</td>
<td>5±5</td>
<td>17±5*</td>
<td>39±5**</td>
<td>89±5**</td>
<td></td>
<td></td>
</tr>
<tr>
<td>4. Hip adductor machine</td>
<td>1±5</td>
<td>13±5</td>
<td>35±5**</td>
<td>85±5**</td>
<td></td>
<td></td>
<td></td>
</tr>
<tr>
<td>5. Sliding hip adduction/adduction</td>
<td>11±5</td>
<td>34±5**</td>
<td>83±5**</td>
<td></td>
<td></td>
<td></td>
<td></td>
</tr>
<tr>
<td>6. Isometric adduction with a ball between the ankles</td>
<td>23±5**</td>
<td>72±5**</td>
<td></td>
<td></td>
<td></td>
<td></td>
<td></td>
</tr>
<tr>
<td>7. Side-lying hip adduction</td>
<td>49±5**</td>
<td></td>
<td></td>
<td></td>
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<td></td>
</tr>
</tbody>
</table>

*p<0.05 and **p<0.01 (Bonferroni corrected).

Values are reported as the difference of least square means in % nEMG± SE. Exercises are listed according to the level of peak nEMG of the dominant adductor longus with peak nEMG stated in brackets. nEMG=normalised electromyography.
Our findings show a significant asymmetry in muscle activation between legs in three exercises. This information can assist in the selection of exercises, for example, if a differentiated training load between legs is desired. We found no significant differences in muscle activation between legs in the symmetrically performed exercises. Previous research has documented strength asymmetries between legs in elite soccer players. However, there is no indication that this has any influence on our EMG findings in the symmetrical exercises.

The muscle activity of the secondary muscles (abdominals and gluteals) all show values of less than 49% nEMG. Consequently, the included exercises are not ideal for strength training of these specific muscle groups in healthy athletes. In comparison, other studies have found values at 16–32% nEMG and 39–64% for the external abdominal oblique and rectus abdominis, respectively, during abdominal crunch exercises. Both considerable movement and stabilisation of the trunk are required in soccer, especially during kicking, and recurrent stress on the abdominal muscles during soccer has been suggested to be involved in the aetiology of groin pain.

Therefore, choosing exercises with a high abdominal activation also seems relevant in relation to groin injuries. To target the abdominal muscle-tendinous structures to some extent, through the exercises included in the present study, the Copenhagen Adduction exercise seems preferred, as it shows the highest values for the abdominal muscles reaching 36% and 40% peak nEMG for the external abdominal oblique and rectus abdominis on the non-dominant side, respectively.

Limitations

The present study was conducted on male soccer players only and therefore limits the generalisation to this group. Consequently, we cannot conclude that the results are applicable to females, other types of athletes, players with pathologies or the general untrained population.

Surface EMG is subject to various limitations, as the EMG signal is influenced by factors such as thickness of tissue layers, possible cross talk, electrode shifting, changes in muscle tissue conductivity, etc. To reduce variability as much as possible, the same tester conducted the preparation of all participants using a precisely described placement of electrodes. Additionally, this study utilised standardised reference contractions. Furthermore, a 500 ms RMS window was used in the analysis to minimise the influence of rapid changes in muscle activity during the repetitions.

The literature lacks consistency in the description of MVCs for the adductor longus. Consequently, the MVC test position was chosen because the majority of the exercises in the present study are performed with the hips and knees straight. We found that the MVC had a lower peak EMG than some of the exercises. Therefore, the results of the present study might not be reproducible when using a different MVC test for normalisation. Based on the results of this study, an isometric hip adduction with hip and knee flexion and a ball between the knees should be considered as an MVC in future studies concerning adductor longus EMG measurements.

Two ICC measurements for the dominant adductor longus showed less than excellent values. These were from the isometric exercises. We did not find any significant differences in peak nEMG between legs in the isometric exercises, and as the ICC values for the EMG activity in the non-dominant leg in the isometric tests were excellent (0.89), we do not consider the lower ICC values for the dominant leg to have a significant influence on our findings. This could be due to the large sample size reducing this possible measurement variation.

The use of a Bonferroni correction in the post-hoc analysis is a very conservative approach and increases the risk of type 2 errors, that is, false negatives. The post-hoc analyses show significant differences for the three exercises with the lowest peak nEMG, but not between the five exercises with the highest peak nEMG. These five exercises were, however, all within 10% nEMG, which was predetermined as clinically irrelevant. Thus, a possible type 2 error is not considered to be of clinical relevance.

CONCLUSION

Specific hip adduction exercises can be graded by exercise intensity, providing athletes and therapists with the knowledge to select appropriate exercises during different phases of prevention and treatment of groin injuries. The Copenhagen Adduction and the hip adduction with an elastic band are dynamic high-intensity exercises, which can easily be performed at any training facility and therefore seem relevant to include in future prevention and treatment programmes.

What this study adds

- Specific hip adduction exercises display different levels of adductor longus muscle activity, indicating differences in exercise intensity between specific exercises.
- This enables a deliberate choice of exercises based on intensity, which is relevant in different phases of prevention and treatment of groin injuries.
- The Copenhagen Adduction exercise and the hip adduction exercise with an elastic band are dynamic high-intensity exercises with limited or no equipment. Therefore, they have great potential for on-field prevention and treatment programmes.


EMG evaluation of hip adduction exercises for soccer players: implications for exercise selection in prevention and treatment of groin injuries

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